SIMULATED EFFECTS OF SYMPATHETIC STIMULATION ON THE ACTION POTENTIAL OF VENTRICULAR CARDIOMYOCYTES

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Abstract: Cathecholamines increase heart rate and contraction force. This effect is mainly mediated by their interaction with the β -adrenergic receptor (β -AR) and its downstream ability to modulate Ca²⁺ cycling and fluxes of a number of ions through specific channels across the cell membrane. The complex nature and broad cellular influence of the β-AR signaling cascade suggest that an integrative modelling approach is appropriate to size the relative weight of each of the single mechanisms by which *β*-adrenergic inputs modulate whole-cell action potential (\overrightarrow{AP}) and Ca^{2+} handling in cardiac myocytes. To this aim, the ventricular AP was simulated by using the Luo-Rudy model and the transmural heterogeneity of the AP (epicardial, midmyocardial and endocardial cells) was reproduced. The β-AR stimulation was modelled bv incorporating its effects on L-type Ca^{2+} current, phospholamban, I_{Kr} , I_{Ks} and Na^+-K^+ pump. Simulation of β-AR stimulation showed significant changes in the AP and in Ca²⁺ handling, depending on the cell type and on the levels of ion fluxes alterations due to β-adrenergic inputs. Notably, the earlydelaved-afteroccurrence of and depolarizations (EADs and DADs respectively) was reproduced. EADs and DADs are suggested as mechanisms responsible for the arrhythmogenic effect of the adrenergic stimulation.

Introduction

The sympathetic neurotransmitter norepinephrine and the adrenal hormone epinephrine (both referred to as cathecholamines) increase the force of contraction and the rate of relaxation of cardiac muscle. These actions are initiated by β -adrenergic receptor (β -AR) coupling with the stimulatory G-protein and subsequent stimulation of adenylyl cyclase, which synthesizes the classical second messenger cyclic AMP (cAMP). cAMP activates cAMP-dependent protein kinase (PKA), leading to the phosphorylation of a wide spectrum of target proteins directly involved in excitation contraction (EC) coupling.

Upon depolarization, Ca^{2+} flowing into the cell through the L-type calcium channels leads to Ca^{2+} release from the sarcoplasmic reticulum (SR). This influx of Ca^{2+} during subsequent beats also loads the SR and participates in activation of myofilaments. Thus, controlling the amount of Ca^{2+} influx through the cell membrane the L-type calcium current $(I_{Ca(L)})$ is a key determinant of contractility. β -adrenergic agents such as isoproterenol have been shown to enhance $I_{Ca(L)}$, through the PKA-induced phosphorylation of the channel [1].

Phospholamban (PLB) is the main regulator of the Ca^{2+} -ATPase activity in cardiac SR. β -adrenergic stimulation increases the phosphorylation of this regulatory protein [2], causing phospholamban to dissociate from the SR Ca^{2+} -ATPase, thus increasing the rate of Ca^{2+} uptake (I_{up}) into the SR.

The slow component of the delayed-rectifier K^+ current (I_{Ks}) plays an important role during the repolarization in the human heart. The β -AR agonist isoproterenol has been shown to increase 2- to 3-fold the current magnitude of I_{Ks} [3].

The rapid component of the delayed-rectifier K^+ current (I_{Kr}) is another critical repolarizing K^+ current. It has recently been demonstrated that I_{Kr} is regulated by β -adrenoreceptor stimulation via a PKA dependent pathway [4]. I_{Kr} is reduced by PKA activation.

Ion transport mediated by the Na⁺-K⁺ pump has been suggested to be stimulated by either norepinephrine and isoproterenol. This increase in the Na⁺-K⁺ current (I_{NaK}) has been shown to be mediated by β -AR activation [5].

Sympathetic stimulation modulates physiological cardiac activity, but also is involved in many pathophysiological conditions, such as Long QT syndrome and cardiac ischemia. Congenital forms of LQTS have been shown to be sensitive to increased sympathetic nervous system activity or to exogenously administration of cathecolamines. Notably, life-threatening arrhythmias can be triggered by sympathetic activation. Accordingly, β -adrenergic blockade has long been accepted as front line therapy for LQTS.

However, the outcome of β -AR activity is the result of coordinated modulation of several ionic fluxes, so that it may result difficult to size their relative importance. In the present study, a mathematical model of ventricular AP was used to investigate the effects of the β -adrenergic inputs on the cardiac electrical activity and contractility at the cellular level. In particular, different levels of alteration of $I_{Ca(L)}$ and I_{up} were analysed.

Materials and Methods

The ventricular AP was simulated by using the Luo-Rudy (LRd) model (Fig. 1) [6] implemented in Simulink 5 (The MathWorks. Inc- Natick, Mass; USA). The action potential (V_m) was reconstructed by numerically solving the differential equation (1) describing the rate of changes of the membrane potential:

$$\frac{dV_m}{dt} = -\frac{1}{C_m} (I_{pacing} + \sum_i I_i)$$
(1)

where C_m is the membrane capacitance, I_{pacing} is a stimulus current, and $\Sigma_i I_i$ includes all currents carried by voltage-gated ion channels, exchange proteins and pumps. Ionic processes are formulated on the basis of experimental data obtained mostly from the guinea pig. The model also accounts for processes that regulate the dynamic concentration changes of Ca²⁺: uptake into the SR, release of Ca²⁺ from the SR and Ca²⁺ buffering by troponin and calmodulin (in the cytosol) and calsequestrin (in the SR).



Figure 1: Schematic diagram of the Luo-Rudy ventricular cell model

Table 1: Simulated alterations of ion currents due to β -AR stimulation. Values are the percentage of the baseline current. In parenthesis the bibliographic references are indicated.

Current	Case 1	Case 2
I _{Ca(L)}	250 [1]	200 [1]
I _{up}	140 [2]	300 [2]
I _{Kr}	30 [4]	
I _{Ks}	250 [3]	
I _{NaK}	120 [5]	

In this study, as a difference from the original LRd formulation the Hodgkin-Huxley formulation of I_{Na} was substituted with a more detailed Markov model [7], and the transient outward current I_{To} described by Dumaine et al. [8] was added. Simulations were performed considering individually the epicardial (Epi), midmyocardial (M) and endocardial (Endo) cells, differentially simulated by assigning three distinct expression levels of maximal conductance of the transient outward current (G_{To}) [8] and three ratios of slow (I_{Ks}) vs. rapid (I_{Kr}) components of the delayedrectifier potassium current [9]. In Epi cells G_{To} was set to 1100 S/F and the density ratio of I_{Ks} to I_{Kr} was set to

63. In M cells, $G_{To} = 500$ S/F and $I_{Ks}/I_{Kr} = 23.3$. In Endo cells, $G_{To} = 50$ S/F and $I_{Ks}/I_{Kr} = 29.6$. Maximal conductance of L-Type calcium current was decreased by 20% with respect to the original LRd formulation in all cells [8].

 β -AR stimulation was modelled by incorporating PKA-mediated effects on L-type Ca²⁺ channels, PLB, I_{Kr}, I_{Ks} and Na⁺-K⁺ pump. The maximal conductance of each channel was modified in order to mimic the alteration of the phoshorylation state. Two different profiles of alteration of ion fluxes were simulated (Table 1).

Pacing was obtained by a current pulse train (pulses of 1 ms in duration) of 50 A/F in amplitude with frequency of 80 bpm. Rosenbrock variable step algorithm (max step 0.1 ms) was used to numerically solve the model equations. In order to ensure a steady state condition, 180 s long simulations were performed; all the data shown refer to the last beat.

Results

When the case 1 is simulated, the response of cardiac cell to β -AR stimulation is related to the myocardial layer where the cell belongs. In fact, AP shape and duration of Endo and Epi cells were not modified by the sympathetic stimulation (Fig.2, upper and lower panels), while M cell was dramatically influenced. Notably, the repolarization of the cell in this layer was retarded and early-after-depolarizations (EADs) occurred (Fig.2, middle panel). In our simulations these latter are mainly due to the reactivation of the depolarizing current $I_{Ca(L)}$ (not shown), determining a net inward current in the plateau phase.



Figure 2: Simulated APs corresponding to condition 1.

At the same time, the enhanced Ca^{2+} uptake and the increased $I_{Ca(L)}$ concentrate Ca^{2+} into the SR and hence

enlarge the size of the Ca²⁺ transient observed during β -adrenergic stimulation in all cell types (Fig.3).



Figure 3: Simulated Ca^{2+} transients corresponding to condition 1.

Also when a further increase in the rate of Ca^{2+} uptake into the SR was simulated (case 2), M cells showed a prolonged AP with respect to control condition, whereas Epi end Endo cells showed only slight changes (Fig. 4). Notably, in all cell types delayed-after-depolarizations (DADs) arose after full repolarization (Fig. 4). DADs are linked to spontaneous Ca^{2+} releases from the SR due to Ca^{2+} overload in this compartment, which in turn reflects the enhanced rate of Ca^{2+} uptake. In our simulations, the late increase in the intracellular Ca^{2+} concentration (Fig.5) induces a large inward current carried by the Na⁺/Ca²⁺ exchanger (not shown). This late depolarizing current is responsible for the observed oscillations of the membrane potential.



Figure 4: Simulated APs corresponding to condition 2.



Figure 5: Simulated Ca^{2+} transients corresponding to condition 2.

Discussion

Although adrenergic stimulation has been described as the responsible for the development of cardiac arrhythmias in many pathological conditions, such as the Long QT (LQT) Syndrome and cardiac ischemia, the cellular basis for the arrhythmogenic actions of the sympathetic nervous system is poorly understood. β adrenergic control of cardiac contractility is believed to be dominated by PKA phosphorylation of the L-type Ca²⁺ channel and PLB, important players in the regulation of Ca²⁺ dynamics and transport. In the present study, a mathematical model of ventricular AP was used to analyse the role of PKA phopshorylation of L-type Ca²⁺ channels and PLB in modulating the wholecell response to β -adrenergic inputs in different ventricular layers.

Action Potential. The response of AP to β adrenergic stimulation largely depends on the balance between the inward and outward currents active during the plateau phase. In our simulations this balance is shifted according to the cell type. In Endo and Epi cells, an increase in the outward repolarizing current, due to a relatively large increase of $I_{\text{Ks}},$ vs. an increase in the inward depolarizing current, I_{Ca(L)}, makes the AP insensitive to β -adrenergic stimulation (Fig. 2, upper and lower panels), whereas the prolonging of the M cell AP (Fig. 2, middle panel) reflects the shift of the balance in favour of $I_{Ca(L)}$. In detail, if $I_{Ca(L)}$ is sufficiently enhanced, the prolonged AP is accompanied by induction of EADs. These results are consistent with experimental data by Burashnikov and Antzelevitch [10], who showed that isoproterenol (in the presence of I_{Ks} blockade) significantly prolonged the AP of M, and caused little change in Epi and Endo cells. However, the study did not show induction of EADs by isoproterenol. In fact, the M cell has been reported to have an intrinsically smaller I_{Ks} among the three transmural cell

types [9]. In general, a defect in I_{Ks} (e.g. LQT Syndrome) could offset the balance between depolarizing and repolarizing currents, thus creating the bases for cardiac arrhythmias to develop. In the LQT1 model (reduced I_{Ks}), Shimizu and Antzelevitch showed that isoproterenol prolongs the AP of the M cell because of I_{Ks} (outward current) reduction to levels at which $I_{Ca(L)}$ (inward current) predominates. On the other hand, higher levels of I_{Ks} in Epi cell (even in the presence of the I_{Ks} blocker chromanol 293B) account for the reduced duration of its AP as a response to the β -agonist [11].

When the I_{up} activity was further increased (condition 2), DADs occurred in all cell types (Fig. 4). The induction of DADs by isoproterenol has been reported by Song *et al.* [1] and Burashnikov and Antzelevitch [10]. These oscillations of the membrane potential are caused by a transient outward current (I_{Ti}), which is active in the late phase of the cardiac cycle. In our simulations, this current results to be carried by the Na⁺/Ca²⁺ exchanger (not shown), as it has already been shown by Zeng and Rudy [12].

Our results suggest an explanation for the role of sympathetic activity as a trigger for cardiac arrhythmias. In fact, when EADs and DADs are sufficiently large to depolarize the cell membrane to its voltage threshold, they give rise to triggered action potentials, which are believed to underlie some forms of extrasystolic activity and tachyarrhythmias.

 Ca^{2^+} handling. In all cell types, the simulation of sympathetic stimulation is accompanied by a large increase in the intracellular Ca²⁺ concentration (Figg. 3 and 5), accounting for the well known inotropic response to β -adrenergic inputs. The observed changes depend on the increase in Ca²⁺ content in the SR, which in turn is due to the augmented rate of Ca²⁺ uptake by the SR and the increased size of I_{Ca(L)}. In addition, when the rate of Ca²⁺ uptake is further enhanced, oscillatory release of Ca²⁺ from the SR was also observed (Fig. 5), in agreement with Song *et al.* [1]. From the mechanical point of view, this spontaneous release, due to Ca²⁺ overload in the SR, is associated with aftercontractions.

Conclusions

In the present analysis, the effects of β -stimulation on ventricular AP and Ca²⁺ cycling were investigated by using a computational model of the cardiac electrical activity. Depending on the levels of expression of I_{Ca(L)} and I_{up}, EADs and DADs were suggested as mechanisms responsible for the arrhythmogenic effect of β -adrenergic stimulation. In addition, it is proposed that the increase in these fluxes also accounts for the elevated intracellular Ca²⁺ responsible for the augmented cardiac contractility.

References

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